

MRISIM.JL: TOOLBOX FOR SPIN-LEVEL SIMULATIONS

PROJECT PRESENTATION

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MOTIVATION

“Being as far as possible from models”

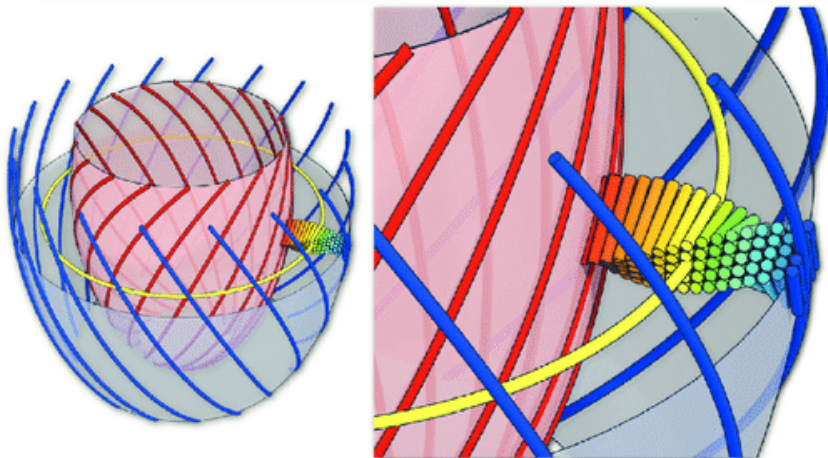
“Being as far as possible from models”

- Closer to reality
- Applicable to multiple problems
- Can help to test novel methods

“Being as far as possible from models”

- Closer to reality
- Applicable to multiple problems
- Can help to test novel methods
- Speed (GPU and parallelization)

Other simulators were not **general** enough
to match our needs



For this we used Julia: **Fast and easy to write**

What makes **julia** great?

✓ Java
Δ Python (Cython, etc)
Δ R (vectorized)

When coded well, it
is very fast

Δ Java (not concise)
✓ Python
Δ R (only R code,
not C or C++)

Clear, concise
code that can easily
be changed

Δ Java (not really)
✓ Python
Δ R (only vectorized)

Great ability to mix
loop based &
matrix/vector
operations

Examples in our simulator:

Gradient and Sequence objects

```
## Grad.jl
struct Grad
    A::Real #Amplitud [T]
    T::Real #Duration of gradient [s]
    DAC::Bool #If we take data during that period
end

## Sequence.jl
struct Sequence
    GR::Array{Grad,2} #Sequence in (X, Y and Z) and Time
end
```

Scalar and matrix multiplication

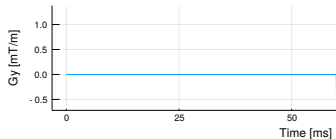
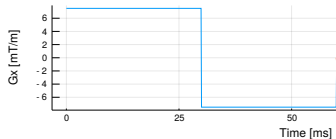
```
## Grad.jl: Gradient operations
```

```
*(x::Grad, α::Real) = Grad(α*x.A,x.T,x.DAC)
```

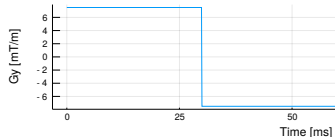
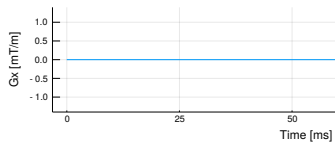
```
*(x::Array{Grad}, A::Matrix) = [sum(x[i,:]*A[j,i] for i=1:size(x,  
    1))[k] for j=1:size(x,1), k=1:size(x,2)] #matrix-mult
```

```
## Sequence.jl: Sequence operations
```

```
*(x::Sequence, A::Matrix) = Sequence(x.GR*A)
```



$$\cdot R_z(\theta) =$$



Pulse programming example

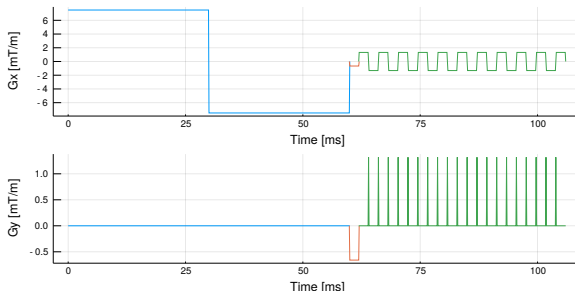
```
## Sequence.jl: Sequence operations
```

```
+(x::Sequence, y::Sequence) = Sequence([x.GR y.GR])
```

```
## Example.jl
```

```
DIFF = Sequence([Grad(G,T) Grad(-G,T); #PGSE on x-dir  
                Grad(0,T) Grad( 0,T)])
```

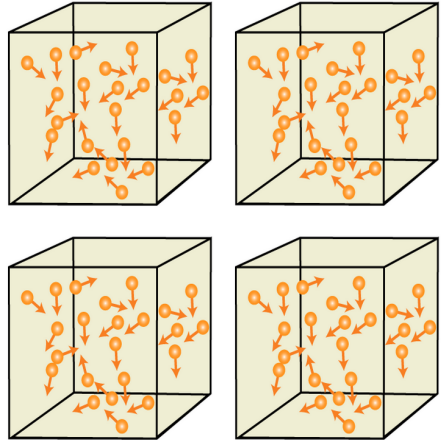
```
SEQ = q*DIFF*rotz( $\theta$ ) + PHASE + EPI
```



SIMULATOR

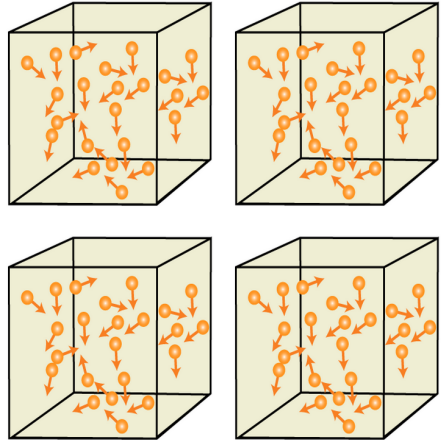
After excitation the signal
depends on the spin phases

$$\phi_n(\mathbf{x}, t) = \gamma \int_0^t \left(\underbrace{\mathbf{x}_n(\tau) \cdot \mathbf{G}(\tau)}_{k\text{-space encoding including motion.}} + \underbrace{\delta B(\mathbf{x}_n^0)}_{\text{off-resonance}} \right) d\tau.$$



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$$\mathbf{x}_n(t^{k+1}) = \underbrace{\mathbf{x}_n^0}_{\text{Position}} + \underbrace{\boldsymbol{\eta}(\mathbf{x}_n^0, t^k)}_{\text{Diffusion}} + \underbrace{\mathbf{u}(\mathbf{x}_n^0, t^k)}_{\text{Displacement}}$$

The signal equation considers all relevant effects

$$S(t^k) = \sum_{n=1}^{N_s} m(x_n^0) \exp\left(-t^k/T_2(x_n^0) + i\Delta\omega(x_n^0)t^k\right) \exp\left(i\gamma\Delta t \sum_{l=0}^k x_n(t^l) \cdot G(t^l)\right)$$

1. Proton density,
2. T₂-decay,
3. Position, motion, flow and Diffusion,
4. Off-resonance (T₂^{*}, concomitant gradients, etc.).

The simulator pipeline has **three** main objects



SpinLab



Scanner



Pulses



Phantom



Simulator

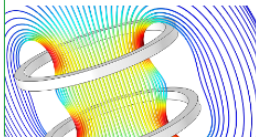


Recon.

Scanner

Description of the hardware limitations, such as B_0 , B_1 , G_{\max} , and S_{\max} .

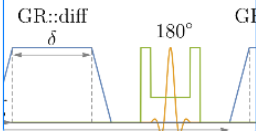
It is also possible to include field imperfections as an additional term $\Delta B(\mathbf{x}, \mathbf{G})$.



Pulses

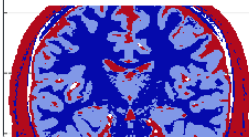
Sequence of pulses, including the gradients $\mathbf{G}(t)$ and RF $B_{1,e}(t)$ signals.

It can also visualize the k -space of the acquisition.



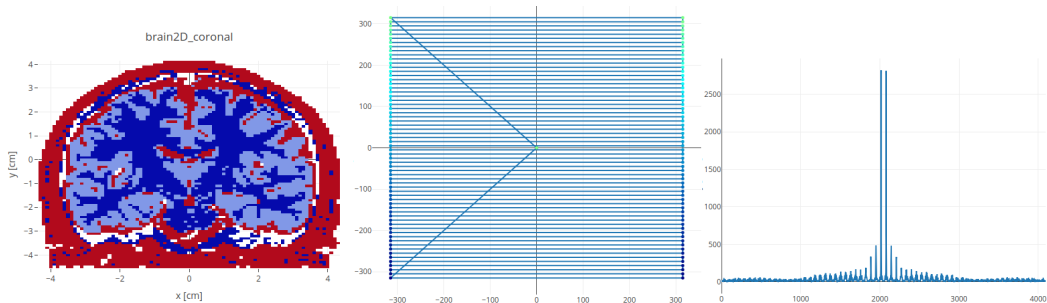
Phantom

Definition of the phantom model, includes information about the proton density ρ , T1, T2, off-resonance $\Delta\omega$, diffusion, and displacement field $\mathbf{u}(\mathbf{x}, t)$.



Run simulation!

Phantom→Scanner+Sequence→Signal



EXAMPLES

E1) Brain phantom with different TEs

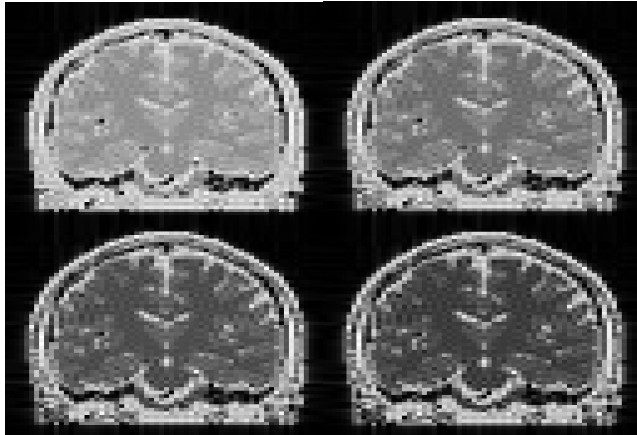
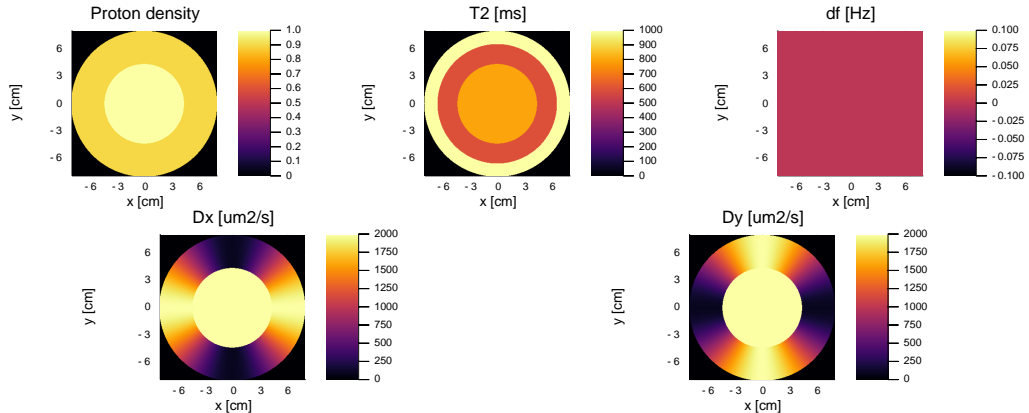


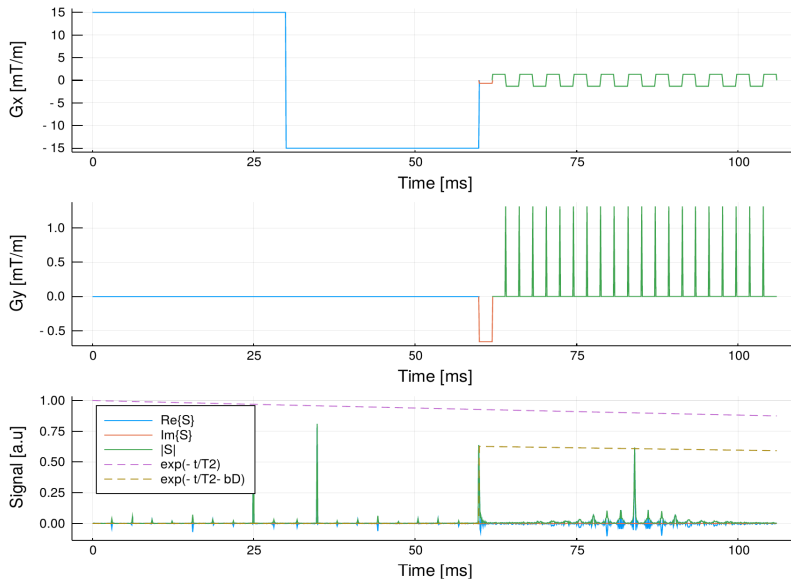
Figure 1: EPI acquisition with $TE = \{16, 30, 60, 80\}$ ms.

E2) Cardiac diffusion on static phantom

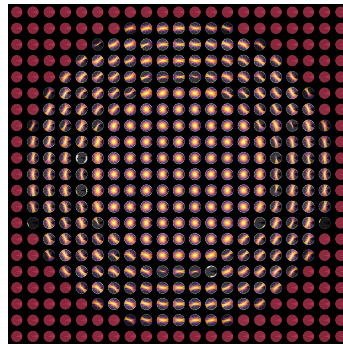
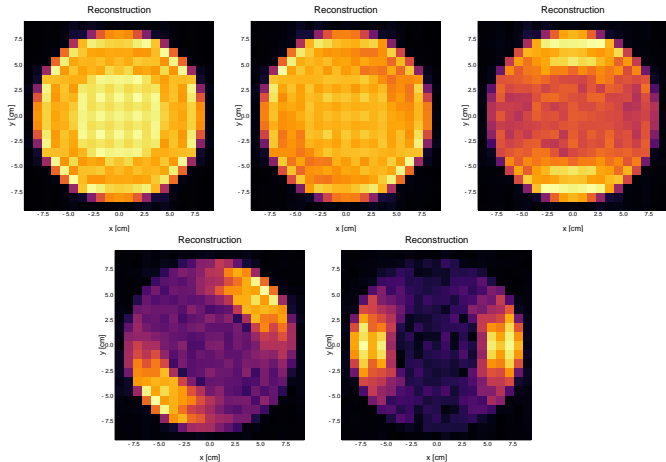
The phantom was defined by the following fields:



The sequence used was a PGSE



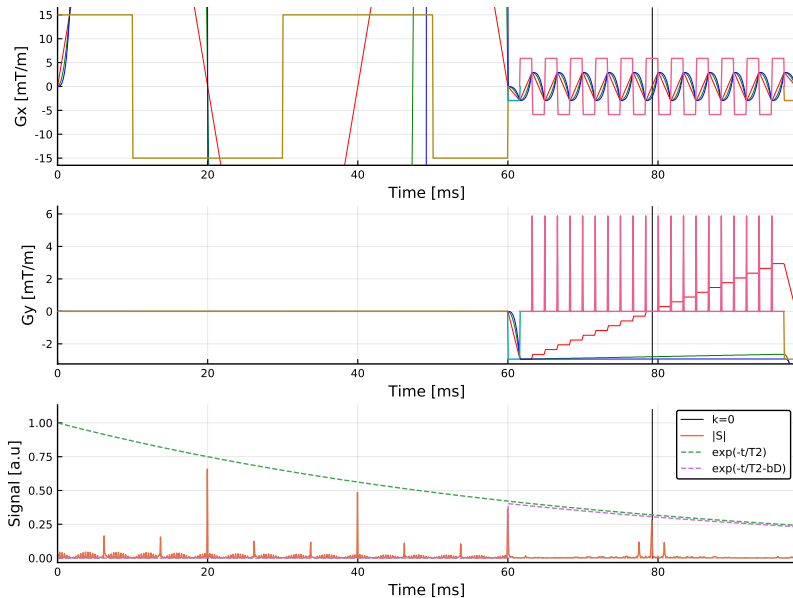
We acquired images with different diffusion encodings (left)
and reconstructed the diffusion propagators (right)



E3) Moment-compensated cardiac diffusion

- It was dynamic, with one diffusion encoding direction.
- The displacement field mimics a real human ventricle.

The sequence was a moment-compensated PGSE



Resulting images **without** and **with** moment-compensation

DEMONSTRATION

Acknowledgments

Millenium Science Initiative of the Ministry of Economy, Development and Tourism, grant Nucleus for Cardiovascular Magnetic Resonance.



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